

Radiolabeled Nanoparticles as Dual-Modality Imaging Agents

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Cancer is a broad group of various diseases, all involving unregulated cell growth. In cancer, cells divide and grow uncontrollably, forming malignant tumors, and invade parts of the body.

In 2012 approximately 14 million cancers were diagnosed and 8.2 million people died of cancer worldwide.

Medical tests for suspected cancer patients

Blood tests



• Endoscopy



Imaging techniques



Imaging Techniques

Non ionizing radiation

≻Optical Imaging



>UltraSonography



lonizing radiation



Computed Tomography (CT)



Magnetic Resonance Imaging (MRI)



➢Nuclear Medicine Techniques (PET and SPECT)



Before Therapy

PET Scan After Therapy



Multimodality Imaging Techniques

No single imaging technique is perfect...

- SPECT/CT
- PET/CT
- SPECT/optical
- PET/optical
- CT/optical
- MRI/optical
- SPECT/MRI
- PET/MRI

The combination of two or more imaging techniques can therefore offer synergistic advantages over any modality alone.



PET/CT imaging of bone cancer with hot spots on the ribs and spine



SPECT/CT imaging of liver cancer with hot spots on the liver

Dual modality PET/MRI or SPECT/MRI probes would provide us images which combine the high spatial resolution of MRI with the high sensitivity of NMT

Hybrid PET/MR Systems

Simultaneous PET/MR scanners

Sequential PET/MR scanners

PET and MRI are largely complementary techniques and the combination would certainly be a 'marriage of convenience' – with PET (exceptionally sensitive but with poor spatial resolution) synergistically linked to MRI (giving supremely high-resolution anatomical information in the submillimetre range).

Nanoparticles as dual-modality imaging agents

The development of hybrid SPECT/MRI and PET/MRI systems has triggered an unprecedented quest for novel dual-modality imaging agents for application to such systems. It is interesting to note that few SPECT/MRI or PET/MRI agents have been reported but, now, with the development of suitable equipment, there is huge scope for the development of hybrid SPECT/MRI and PET/MRI probes.



Surface functionalization of nanoparticles allows them to "behave" as dual-modality imaging agents both for SPECT/MRI and PET/MRI applications

Commonly-used Radioisotopes for Nanoparticle Radiolabeling

Radionuclide	t _{1/2} (h)	Emission type (%)	Energy (keV)	Mode of Generation	Radiolabeling Methods
^{99m} Tc	6.02	γ, ΙΤ	140	⁹⁹ Mo/ ^{99m} Tc generator	Coordination Chemistry
¹¹¹ In	67.2	Auger e ⁻ , EC	172,247	Cyclotron	Coordination Chemistry
⁶⁷ Ga	78.1	γ, EC	93,185,300	Cyclotron	Coordination Chemistry
¹⁸ F	1.83	β ⁺ (97), EC (3)	635	Cyclotron	Direct (Nucleophilic or Electrophilic) or Indirect (prosthetic) Labeling
⁶⁴ Cu	12.9	β+(19.3), β ⁻ (39.6), EC (45)	573,654	Cyclotron	Coordination Chemistry
⁶⁸ Ga	1.14	β ⁺ (90), EC (10)	770,1880	⁶⁸ Ge/ ⁶⁸ Ga generator	Coordination Chemistry
124	76.8	β ⁺ (25), EC (75)	790,1530,2130	Cyclotron	Nucleophilic Halogen Exchange Chemistry

Nanoparticle Radiolabeling

Radiolabeling of nanoparticles with metallic radionuclides



T.L.Ross et al, Radiolabeling of nanoparticles and polymers for PET imaging, Pharmaceuticals 2014; 7(4): 392-418

Nanoparticles as dual-modality PET/MRI imaging probes

A. Schematic diagram of an integrin $a_v b_3$ -targeting ⁶⁴Cu-DOTA-IO-RGD PET/MRI dual-modality probe

B. A two-dimensional projection micro-PET image of a mouse bearing an integrin $a_v b_3$ -positive U87MG tumor at 4 hours postinjection of the probe.

C. T2-weighted MRIs of mice before and

D. 4 hours after intravenous injection of the probe.

The arrow indicates the tumor

Lee HY, Li Z, Chen K, et al. PET/MRI dual-modality tumor imaging using arginine-glycine-aspartic (RGD)-conjugated radiolabeled iron oxide nanoparticles. J Nucl Med 2008;49:1371–9





Nanoparticles as dual-modality PET/MRI imaging probes



Simultaneous PET/MR images of the ¹¹C-labeled SPIO NPs in a mouse using a 9.4 T MRI small animal scanner.

Top row: MRI images show loss of signal from the accumulation of SPIO NPs in the liver.

Middle row: PET images
 which result from C-11 positron
 decay show the accumulation of
 ¹¹C-labeled SPIO NPs in the liver.

Bottom row: Fused PET/MR images show the exact correspondence of the two signals.



Sharma R. et al, "Carbon-11 radiolabeling of iron-oxide nanoparticles for dual-modality PET/MR imaging", Nanoscale, 2013, 5, 7476

Nanoparticles as dual-modality PET/MRI imaging probes

Chelator-free radiolabeling of iron oxide nanoparticles with a silica shell.

In vivo mouse images of:

- (a) 10 MBq/50 µg Fe of ⁶⁸Ga labeled iron oxide nanorods, fused PET-CT coronal slice image showing areas of main organ uptake at 80–90 minutes post-injection
- (b) 10 MBq/50 μg Fe, T₂
 weighted MR image at 90
 minutes post-injection
- (c) control mouse without nanoparticle administration, T2 weighted MR image at 90 minutes post-injection
- (d) time-activity-curve for major organs from PET image after administration of 10 MBq/50 µg Fe.



Burke, B. P. et al 2015. "Chelator free gallium-68 radiolabelling of silica coated iron oxide nanorods via surface interactions", Nanoscale, 2015, 7, 14889-14896.

Nanoparticles as dual-modality SPECT/MRI imaging probes



SPECT-MR IMAGING AGENT

Rafael T. M. de Rosales et al, ^{99m}Tc-Bisphosphonate-Iron Oxide Nanoparticle Conjugates for Dual-Modality Biomedical Imaging, Bioconjugate Chemistry 2011; 2: 455-465

Bevacizumab-conjugated SPIONs



Schematic representation of bevacizumab-conjugated ferromagnetic nanoparticles (Bc-FNs) and their binding to M165 cancer cells overexpressing the VEGF-165 isoform.

Binding efficiency of Bevacizumab-conjugated SPIONs

- M165 cells were plated in 6-well plates for 24 h
- Bevacizumab conjugated-FNs were added at predetermined concentrations (1 mM Fe and 5 mM Fe per well)
- After I h incubation at 4 °C, the supernatant was removed and the cells were carefully washed with PBS
- The cells were incubated with goat antihuman IgG-FITC for 2 h, washed using PBS three times, treated with paraformaldehyde (4%, 0.5 mL) for 10 min to fix the cells, and then washed with PBS.
- The cells were visualized with fluorescence microscopy





Fluorescence microscopy of Bc-FN bioconjugates incubated with M165 cells overexpressing the VEGF-165 isoform. Vivid green fluorescence indicative of successful VEGF-165 targeting is detected for M165 cells treated with the Bc-FNs (b), as opposed to the same cells treated with a control conjugate (a)

Radiolabeling of Bevacizumab-SPIONs with Technetium-99m: ex vivo and in vivo assessment





Passive accumulation of NPs-DMSA- 99m Tc showed minimal tumor uptake (2.1% ± 0.34% ID/g vs 1.9% ± 0.2% ID/g at 2 and 24h, respectively)



Scintigraphy of NPs-DMSA-SMCC-bevacizumab-^{99m}Tc showed a clear visualization of the tumor, while for NPs-DMSA-^{99m}Tc the tumor could not be visualized.

AGulX Preclinical Multimodal Probe Theragnostic Nanoparticles MRI-SPECT/PET-Fluorescence-Therapy





Lux F., et al, "Ultrasmall Rigid Particles as Multimodal Probes for Medical Applications", Angew. Chem. Int. Ed. 2011, 50, 1–6

Ultrasmall size 4±1 nm – renal excretion MW 8.5±2 kDa

Polysiloxane composition Easy further functionalization

DOTA (Gd) (MRI-Radiotherapy) FDA approved

Radiometal (M*) chelation PET/SPECT/Therapy

AGulX nanoparticles: Ultrasmall particles for Gd-MRI and ⁶⁸Ga-PET dual-modality imaging

Nanoparticles made of polysiloxane matrix and surrounded by DOTAGA[Gd³⁺] and NODAGA[⁶⁸Ga³⁺] have been synthesized for PET/MRI dual imaging. Characterizations were carried out in order to determine the nature of the ligands available for radiolabelling and to quantify them. High radiolabelling purity (>95%) after ⁶⁸Ga labelling was obtained. MR and PET images demonstrate the possibility to use the nanoparticles for combined PET/MRI scanners. The images show fast renal elimination of the nanoparticles after intravenous injection.



Figure 2: Biodistribution of ⁶⁸Ga-AGuIX in normal mice at 30, 60 and 120 min p.i.



MRI/PET images on the same mouse with AGuIX. MR images of a male mouse (a,b,c), which was injected with Gd-AGuIX, 60 min prior to the MRI exam. We note a definite enhancement of the kidneys (arrows in b and c). Compare with corresponding slices of the kidneys (arrows in a) of a non-injected male mouse, acquired with the same imaging parameters; d) PET/CT image with ⁶⁸Ga-AGuIX.

C. Truillet, P. Bouziotis, C. Tsoukalas, J. Brugière, M. Martini, L. Sancey, T. Brichart, F. Denat, F. Boschetti, U. Darbost, I. Bonnamour, D. Stellas, C.D.Anagnostopoulos, V. Koutoulidis, L.A. Moulopoulos, P. Perriat, F. Lux and O. Tillement, "Ultrasmall particles for Gd-MRI and ⁶⁸Ga-PET dual imaging", Contrast Media and Molecular Imaging, 2015

AGulX nanoparticles: Ultrasmall particles for Gd-MRI and ⁶⁸Ga-PET dual-modality imaging



Metabolite studies of ⁶⁸Ga-AGuIX@NODAGA in tumor (C), blood (D) and urine (E) of tumor-bearing mice, at 60 min post-injection (the pre- and post-purification HPLC curves, (A) and (B) respectively, are given as a reference)

AGuIX nanoparticles:

Ultrasmall particles for Gd-MRI and ⁶⁸Ga-PET dual-modality imaging





Left: T1-weighted MR images of a female mouse before (a) and 60 min after (b) injection of 20 mol Gd-AGuIX@NODAGA.

Right: PET image of a U87MG tumor-bearing mouse injected with ⁶⁸Ga-AGuIX@NODAGA, at 60 min p.i.

Bouziotis P, Stellas D., ThomasE., Truillet C., Tsoukalas C., Lux F., Tsotakos T., Xanthopoulos S., Paravatou-Petsotas M., Gaitanis A., Moulopoulos L., Koutoulidis V., Anagnostopoulos C.D., Tillement O., "⁶⁸Ga-radiolabeled AGuIX nanoparticles as dual-modality imaging agents for PET/MRI guided radiation therapy", Nanomedicine, July 2017

Histopathological studies

A and B: Gross anatomic features of ⁶⁸Ga-AGuIX@NODAGA injected mouse post mortem.

C: PET/CT overlay image verifies the accumulation of ⁶⁸Ga-AGuIX@NODAGA NPs in the tumor. ⁶⁸Ga-AGuIX@NODAGA NPs are also weakly present in the liver.

D: The gross anatomy of the U87MG generated tumor after the excision.

E and F: Low magnification (scale bar = 200 μ m) and high magnification (scale bar = 100 μ m) of the U87MG tumor stained with Hematoxylin and Eosin. It is noteworthy that the ⁶⁸Ga-AGuIX@NODAGA NPs are trapped inside the tumor parenchyma, especially in areas where necrotic features are more evident.

G and H: Higher magnification of the U87MG tumor. With an arrow we indicate the necrotic area and with arrowheads the location of the nanoparticles (scale bar = $25 \mu m$



Bouziotis P, Stellas D., ThomasE., Truillet C., Tsoukalas C., Lux F., Tsotakos T., Xanthopoulos S., Paravatou-Petsotas M., Gaitanis A., Moulopoulos L., Koutoulidis V., Anagnostopoulos C.D., Tillement O., "⁶⁸Ga-radiolabeled AGuIX nanoparticles as dual-modality imaging agents for PET/MRI guided radiation therapy", Nanomedicine, July 2017

AuDTDTPA Gold Nanoparticles

Functionalized gold nanoparticles were applied as contrast agents for both in vivo X-ray and MRI

Synthesis

Encapsulation of gold cores within a multilayered organic shell which is composed of gadolinium chelates bound to each other through disulfide bonds.

MRI contrast enhancement

Due to the presence of Gd ions entrapped in the organic shell

X-ray absorption

This study revealed that

Provided by the gold core Due to the presence of Gd ions entrapped in the organic shell



Alric C., et al, "Gadolinium Chelate Coated Gold Nanoparticles As Contrast Agents for Both X-ray Computed Tomography and Magnetic Resonance Imaging", J. AM. CHEM. SOC. 2008, 130, 5908–5915

these particles suited for dual modality imaging freely circulate in the blood vessels without undesirable accumulation in the lungs, spleen, and liver.

0,6 10.7 min 0.4 Ę 0,2 %ID/g 0,0 10 20 25 5 15 30 Time (min)

AuDTDTPA Gold Nanoparticles

In vitro serum stability study of 68Ga-AGuIX. From left to right:

⁶⁸Ga-eluate

68Ga-Au@DTDTPA-cRGD ⁶⁸Ga-Au@DTDTPA-cRGD/serum stability 20min ⁶⁸Ga-Au@DTDTPA-cRGD/serum stability 120min

Mobile phase: 0.2M KCL pH 3

Key tumor-to-tissue ratios of ⁶⁸Ga-Au@DTDTPA-RGD





Biodistribution studies for ⁶⁸Ga-Au@DTDTPA-RGD radiolabeled nanoparticles







In vivo PET imaging studies



PET/CT imaging of a U87MG tumor-bearing SCID mouse, at 1 h p.i.

The preliminary results of this study warrant the need for further development of Au@DTDTPA-RGD nanoparticles radiolabeled with Ga-68, as a possible dualmodality PET/MRI imaging agent.

Meticulous investigation of the quantities of injected Gd/⁶⁸Ga-Au@DTDTPA needs to be performed, in order to achieve the optimum tracer concentration for both PET (tracer quantities 10⁻⁹ to 10⁻¹² M) and MRI (tracer quantities 10⁻⁴ M) imaging applications.

To sum up...

Although radiolabeled NPs have shown great promise in SPECT/PET imaging of diseases, several challenges need to be addressed to translate the radiolabeled NPs to clinical applications:

- Development of truly tissue-selective targeting NPs without the significant uptake in the mononuclear phagocytic system (MPS) To resolve this issue, the NPs can be designed with optimal surface modifications
- Functionalization of NPs with antibodies, peptides or other targeting ligands that recognize specific receptors or antigens have the potential to increase the target-to-background ratio
- Design considerations (shape, charge, size, surface coating, and dosing) can be manipulated to prolong blood circulation, reduce the nonspecific distribution, and enhance imaging contrast.
- In order to achieve optimal target-to-background contrast in SPECT/PET, good *in vivo* stability of radiolabeled NPs is also required

In conclusion, radiolabeled NPs have shown great promise in SPECT/PET imaging. With the development of hybrid imaging technology, we expect that novel radiolabeled NPs with SPECT/PET along with other imaging modalities will afford accurate and precise assessment of biological signatures in a real-time manner and thus improve disease management.

The design of the appropriate multi-modal imaging probe is vital and any real advances in molecular imaging will be due to the *interdisciplinary efforts* of synthetic chemists, molecular biologists, imaging scientists and clinicians.

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